Diagnostic performance of MRI perfusion and spectroscopy for brainstem glioma grading


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Abstract. – OBJECTIVE: This study investigated the roles of dynamic susceptibility contrast (DSC) perfusion and multivoxel magnetic resonance spectroscopy (MRS) in grading brainstem glioma (BSG).

PATIENTS AND METHODS: Our retrospective study comprised 12 patients, including 6 with pathology verified low-grade BSGs and 6 with high-grade BSGs. We examined differences in age, relative cerebral blood volume (rCBV), regional cerebral blood flow (rCBF), and the metabolite ratios of choline (Cho)/N-acetyl aspartate (NAA) and Cho/creatine (Cr) between these two groups using the Mann-Whitney U test and Chi-square test. Receiver operating characteristic (ROC) curve analysis was used to establish cutoff values and assess their usefulness in grading BSG.

RESULTS: The Cho/NAA metabolite ratio had the strongest preoperative predictive performance for identifying the correct histological grade among BSGs, with an area under the ROC curve (AUC) value of 0.944 (cutoff: 3.88, sensitivity [Se]: 83.3%; specificity [Sp]: 100%), followed by the Cho/Cr ratio (cutoff: 3.08; AUC: 0.917; Se: 83.3%; Sp: 100%), rCBF (cutoff: 3.56, AUC: 0.917; Se: 83.3%; Sp: 100%), rCBV (cutoff: 3.16; AUC: 0.917; Se: 83.3%; Sp: 100%), and age (cutoff: 9.5 years, AUC: 0.889; Se: 100%; Sp: 83.3%).

CONCLUSIONS: rCBF and rCBV values comparing solid tumors with the normal brain parenchyma and the metabolite ratios for Cho/NAA and Cho/Cr may serve as useful indices for establishing BSG grading and provide important information when determining treatment planning and prognosis in patients with BSG.

Key Words: Dynamic susceptibility contrast, Perfusion, Spectroscopy, Brainstem glioma, Grading.

Introduction

Brainstem gliomas (BSGs) account for 10% of all brain tumors in children and 2% of all brain tumors in adults. BSG describes a heterogeneous group of gliomas that vary significantly in histology and prognosis. According to the fifth edition of the WHO classification of central nervous system (CNS) tumors, published in 2021, gliomas can be classified from grade I to IV. In BSG, the histological grade plays a crucial role in treatment planning and is significantly associated with overall survival. Pathology is the gold standard for diagnosing BSG at the cellular level, based on the detection of necrosis, nuclear polymorphism, and endothelial proliferation. However, the performance of biopsies or surgery to characterize or treat brainstem tumors is both challenging and controversial due to the high risks of complications and mortality.

Magnetic resonance imaging (MRI) allows for the noninvasive diagnosis of BSG. MRI can provide a definitive diagnosis in cases of typical diffuse midline glioma, and many brainstem tumors are diagnosed and treated based on imaging findings without histological results. Although the value of MRI for BSG prognosis has been mentioned in prior studies, few studies have examined the role of MRI in BSG grading, which is typically performed using conventional approaches, with a sensitivity (Se) of 46.6% and a specificity (Sp) of 96%. Advanced MRI approaches, such as the combination of magnetic resonance perfusion (MRP), particularly dynamic susceptibility contrast (DSC) perfusion, and magnetic resonance spectroscopy (MRS), have been widely used to investigate the extent of angiogenesis and tumor...
metabolism, factors that are closely correlated with BSG malignancy. However, very few studies have evaluated the role of these sequences in BSG grading, and no studies have reported cutoff values for indicators measured using DSC perfusion or MRS. Therefore, we examined the role of DSC perfusion and MRS in BSG grading and established cutoff values for various indices used in the differential diagnosis of low-grade BSG (BS-LGG) from high-grade BSG (BS-HGG).

Patients and Methods

Study Population

This retrospective study was conducted in the Viet Duc University Hospital Radiology Department, covering the period from June 2019 to May 2022. Twelve enrolled patients (6 with BS-LGG and 6 with BS-HGG) were examined using 3.0 Tesla MRI (SIGNA Pioneer MR, GE Healthcare, Chicago, IL, USA), using the same protocol for all patients (described in Table I) consisting of both conventional and DSC perfusion and multivoxel MRS. All patients subsequently underwent surgery or stereotactic biopsy to obtain a sample for pathological glioma confirmation. The exclusion criteria were patients who received any treatment prior to MRI assessment, such as operative resection, biopsy, or cranial radiotherapy; and patients with MRI results of poor quality, such as the presence of motion artifacts that prevented accurate measurements. This study was reviewed and approved by the Institutional Review Board (Ref: 634/GCN-HDDDNCYSH-DHYHN dated 16 March 2022). Our retrospective study was performed in compliance with the principles outlined in the Declaration of Helsinki. The requirement for informed consent from children and their parents/guardians was waived by the Institutional Review Board of Hanoi Medical University due to the retrospective study, which analyzed anonymized imaging data.

MRI Technique

All research subjects underwent brain MRI evaluations using a 3.0 Tesla scanner system (SIGNA Pioneer MR, GE Healthcare, Chicago, IL, USA) with head coils; the protocol applied to all patients is presented in Table I. Due to the need for prolonged assessments, sedation or general anesthesia is typically necessary to obtain good quality images in children younger than 6 years and some patients with altered mental status. The need for sedation should be assessed on a case-by-case basis. Informed consent was obtained from patients or their parents/guardians for the use of sedation or general anesthesia, and all consents were documented and stored. DSC perfusion was obtained before the administration of contrast agent and the collection of T1-weighted (T1W) contrast images.

Table I. MRI sequences.

<table>
<thead>
<tr>
<th>Sequence</th>
<th>Plane</th>
<th>TR (msec)</th>
<th>TE (msec)</th>
<th>Thickness (mm)</th>
<th>Matrix</th>
<th>FOV</th>
<th>Others</th>
</tr>
</thead>
<tbody>
<tr>
<td>FLAIR</td>
<td>Axial</td>
<td>8500</td>
<td>117</td>
<td>5</td>
<td>184 × 256</td>
<td>240 × 240</td>
<td>IR 2500 ms</td>
</tr>
<tr>
<td>T2 TSE</td>
<td>Axial, coronal</td>
<td>2500</td>
<td>100</td>
<td>5</td>
<td>360 × 288</td>
<td>220 × 220</td>
<td></td>
</tr>
<tr>
<td>T2*SWI</td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
<td>†</td>
</tr>
<tr>
<td>T1 SE</td>
<td>Axial, sagittal</td>
<td>2325</td>
<td>24</td>
<td>5</td>
<td>240 × 240</td>
<td>300 × 224</td>
<td></td>
</tr>
<tr>
<td>T1 SE CE+</td>
<td>Axial, sagittal</td>
<td>2325</td>
<td>24</td>
<td>5</td>
<td>240 × 240</td>
<td>300 × 224</td>
<td>‡</td>
</tr>
<tr>
<td>DSC-MRI</td>
<td>GRE EPI</td>
<td>1250</td>
<td>45</td>
<td>5</td>
<td>88 × 87</td>
<td>338 × 240</td>
<td>§</td>
</tr>
<tr>
<td>MRS</td>
<td>2D multivoxel CSI</td>
<td>8500</td>
<td>144</td>
<td></td>
<td>240 × 240</td>
<td></td>
<td></td>
</tr>
</tbody>
</table>
| Voxel 3D CSI |           | 2000      | 144       |                | Voxel size of 0.9 × 1.6 × 1.2 cm³ |           | 3

TR: Repetition time; TE: Echo time; FOV: Field of view; FLAIR: Fluid-attenuated inversion recovery; IR: Inversion time; T2 TSE: T2-weighted turbo spin-echo; SWI: Susceptibility-weighted imaging; T1 SE: T1-weighted spin-echo; CE+: Contrast enhancement; DSC-MRI: Dynamic susceptibility contrast perfusion magnetic resonance imaging; GRE EPI: gradient-recalled echo-planar imaging; CSI: chemical shift imaging; MRS, magnetic resonance spectroscopy. †Optimal sequence (T2* or SWI) for each patient. ‡Intravenous injection of contrast agent (gadolinium–diethylenetriamine pentaaceta [DTPA]) at 1 ml/kg, with an injection rate of 5 mL/s. §Performed before T1-SE CE+ during the first pass of an intravenous bolus injection of contrast agent (gadolinium–DTPA at 1 ml/kg, with an injection rate of 5 mL/s), 40 acquisition scans with voxel size 2.5 × 2.5 × 5 mm. DSC-MRI was performed using the dynamic T2*-weighted GRE EPI. MRS was performed using 2D multivoxel CSI and Voxel 3D CSI.
**Image Analysis**

MRI results were interpreted according to current radiological criteria by a neuroradiologist with more than 10 years of experience in a blinded manner, with no knowledge of the pathological results, clinical findings, or previous imaging findings. The following regions (Figure 1) were established using the conventional MRI results:

1. **Solid tumor regions** were defined as enhanced sites on T1W contrast-enhanced MRI.
2. **Normal brain parenchyma** was defined as normal contralateral white matter in the cerebral hemisphere or middle cerebral peduncle from the same images used to define the solid tumor.
3. **Cystic degenerating or necrotic tumor regions** were defined as regions with significant hypointensity on T1W images and hyperintensity on T2W images, with no contrast enhancement.
4. **Intratumoral calcifications and hemorrhagic regions** were defined as areas that displayed signal drop-out or blooming artifacts on T2* or post-processed susceptibility-weighted imaging (SWI) and appeared hyperdense on computed tomography images (if available).

Locations containing signals that might interfere with the accurate assessment of signal intensity for the region of interest (ROI) or the voxel placing region were excluded from further analysis (referred to as artifact regions), such as any regions containing tumoral cystic degeneration, calcifications, hemorrhagic regions, intratumoral necrosis, or intratumor vessels. Areas near the skull bone, subcutaneous adipose tissue, and regions with significant variations in magnetic susceptibility were also excluded from the analysis.

MRS was performed for each patient using two-dimensional (2D) multivoxel chemical shift imaging (CSI) or single-voxel 3-dimensional (3D) CSI to identify and quantify metabolites in both the normal brain parenchyma and the intratumoral solid regions. For each patient, a freehand ROI (diameter of 3-4 mm) was manually drawn on a single axial slide containing both the solid tumor and the normal parenchyma free of artifacts (Figure 2). Spectroscopic analysis showed measured the following metabolites: N-acetyl aspartate (NAA) at 2.18-2.01 ppm; creatine (Cr) at 3.15–3.0 ppm; and choline (Cho) at 3.36-3.21 ppm. The Cho/Cr and Cho/NAA ratios were automatically calculated by the software using the integration values of each metabolite in the same spectrum.

The DSC perfusion sequence was acquired during the first pass of a bolus contrast injection, before contrast-enhanced T1W was performed, using dynamic T2*-weighted gradient-recall echo-planar imaging with the same slide thickness as the fluid-attenuated inversion recovery (FLAIR) or T2-weighted (T2W) axial sequence.

**Figure 1.** A 14-year-old male patient presented with a mild headache for 4 months. Axial fluid-attenuated inversion recovery (A) and coronal T2-weighted images (B) show a heterogeneous, hyperintense mass (white arrows) in the brainstem that extends to the upper cervical spine, causing cystic collection in the central canal of the spinal cord, known as syringomyelia. Axial T1-weighted (C) and axial T1-weighted contrast-enhanced (D) imaging at the same level manifest faint heterogeneous enhancement (white arrows).
to assist the juxtaposition of the perfusion results with other pre-contrast sequences. Phase encoding was performed in the anterior-posterior direction for all patients to reduce susceptibility artifacts. The obtained cerebral blood volume (CBV) and cerebral blood flow (CBF) maps were used for further analyses. Two ROIs (diameter of 3-5 mm) were drawn on the solid tumor and normal brain parenchyma at the same level to measure the CBV and CBF values. The selected tumor region was the most hypervascular area that manifested “hot spot areas” of great intensity on the CBV color map, excluding artifact areas. Hemodynamic parameters were calculated from the concentration-time curves, including relative cerebral blood volume (rCBV) and regional cerebral blood flow (rCBF), by normalizing the maximum values obtained for the solid tumor by the values obtained for the normal brain parenchyma (Figure 3).

**Histopathological Examination**

All patients underwent surgery or stereotactic biopsy to obtain a sample for histopathology, which was used to confirm glioma diagnosis. According to the WHO categorization, and to facilitate our statistical analysis, patients were classified as either BS-LGG (WHO grades I and II) or BS-HGG (WHO grades III and IV).

**Statistical Analysis**

Data were analyzed using SPSS 20.0 (Statistical Package for Social Sciences version 20.0, SPSS Inc., Armonk, NY, USA) to determine correlations between MRI characteristics and pathological features. Each parameter was calculated and presented as the mean with both the 25th and 75th percentiles (Q1-Q3) and the standard deviation (SD). Differences between the BS-LGG and BS-HGG were evaluated using the Mann-Whitney U test for age, rCBV, rCBF, Cho/NAA, and Cho/Cre. Categorical variables were compared using the Chi-square test or Fisher’s exact test. The p-values lower than 0.05 were considered significant. Receiver operating characteristic (ROC) curve analysis was performed to estimate the optimal cutoff values for each parameter by maximizing the sum of Se and Sp using the Youden Index. The area under the ROC curve (AUC) was also determined.
Results

The study population included 12 patients (6 males and 6 females; 7 pediatric patients and 5 adults), 6 of whom were diagnosed with BS-LGG and 6 of whom were diagnosed with BS-HGG. The BS-LGG group included 5 patients diagnosed with WHO grade II BSG, whereas the BS-HGG group included 1 patient diagnosed with WHO grade III and 5 patients diagnosed with WHO grade IV BSG. Details are provided in Table II. The demographic characteristics, rCBV, rCBF, Cho/NAA, and Cho/Cr values for the entire cohort are summarized in Table III. No significant difference in sex distribution ($p = 0.248$) was identified between the two groups. Strong correlations were identified between age, rCBV, rCBF, Cho/NAA, and Cho/Cr values and tumor malignancy among BSG patients. The mean age of the BS-HGG group (14.8 ± 17.8 years) was significantly lower than that of the BS-LGG group (35.5 ± 22.9 years, $p = 0.024$). The mean rCBV, rCBF, Cho/NAA, and Cho/Cr values were significantly higher for the BS-HGG group than for the BS-LGG group (Table III).

Figure 3. A 14-year-old male patient presented with a mild headache for 4 months. This image presents an analysis of the same patient from Figure 1 at a lower level, where the tumor manifests “hot spots” on the cerebral blood volume (CBV) color map compared with the normal white matter parenchyma of the cerebellum. Axial T1-weighted contrast-enhanced (A) and axial fluid-attenuated inversion recovery (FLAIR, B) imaging show a diffuse mass in the brainstem (white arrows). The tumoral ROI was placed to capture the greatest intensity on the CBV (B) and cerebral blood flow (CBF) maps (D). Axial FLAIR (E-G) images at the same level show the normal white matter parenchyma (stars) used for placing ROIs on the CBV (F) and CBF maps (H).
ROC curve analyses were performed to determine the ability of each parameter to distinguish BS-HGG from BS-LGG, as shown in Figures 4 and 5, and the AUC and Youden Index were calculated as presented in Table IV. The MRP values, consisting of the Cho/NAA (AUC: 0.944) and Cho/Cr ratios (AUC: 0.917; Figure 4), were better able to differentiate between BS-HGG and BS-LGG than the rCBF (AUC: 0.917), rCBV (AUC: 0.889; Figure 4), or age (AUC: 0.889; Figure 5).

Discussion

Our study included 7 children and 5 adults diagnosed with BSG, including 6 with high-grade tumors and 6 with low-grade tumors. A strong correlation was identified between age and malignancy, as the mean age of the BS-HGG group (14.8 ± 17.8 years) was significantly lower than that of the BS-LGG group (35.5 ± 22.9 years, \( p = 0.024 \)), indicating that more malignant BSGs were more commonly diagnosed in children than in adults. Previous studies have also reported that pediatric cases diagnosed with BSG have a worse prognosis than adult cases diagnosed with BSG\(^1\,\,^5\,\,^6\). According to Reyes-Botero et al\(^3\), among pediatric patients, grade IV is the most common BSG grade, accounting for 50%-60% of all pediatric BSG cases, whereas in adults, up to 80% of diffuse BSG cases are low-grade. However, other studies reported no association between age and histological grade. The study by Moharamzad et al\(^10\) reported mean ages for BS-LGG and BS-HGG groups of 19 and 21, respectively (\( p = 0.37 \)).
Previous studies examining the role of MRI in BSG grading have focused on the application of conventional MRI sequences. Imaging features including tumor location, tumoral extension into adjacent structures, enhancement characteristics, and necrosis have previously been reported to have diagnostic values for BSG grading. The study by Kwon et al examining 20 BSG cases (15 high-grade tumors and 5 low-grade tumors) reported that 100% of high-grade tumors were located in the pons, whereas low-grade tumors were located in many locations. High-grade tumors caused diffuse brainstem enlargement, whereas low-grade tumors were often localized, and glioblastoma (grade IV) was often characterized by necrosis and ring enhancement. The study by Moharamzad et al examining 96 BSG cases revealed that necrosis and heterogeneous enhancement are suggestive characteristics of BS-HGG. However, the correct diagnosis rate using conventional MRI sequences is not sufficient. Rachinger et al examined 46 adult BSG cases and reported that the diagnostic Se and Sp of conventional MRI for identifying BS-LGG were only 62.5 and 46.6%, respectively, and...
the corresponding values for BS-HGG were 58.3 and 61.7%, respectively. In the study by Goda et al\textsuperscript{13}, which included 20 BSG patients, the Se and Sp of conventional MRI for low-grade tumors were 66% and 33%, respectively, and the corresponding values for high-grade tumors were 50% and 50%, respectively. Conventional MRI has certain limitations when applied to BSG grading. Enhancement can be caused by both tumor angiogenesis and the disruption of the blood–brain barrier. In addition, many studies have shown that BS-HGGs may not enhance after contrast injection, whereas some BS-LGGs and non-tumor brainstem lesions may enhance after contrast injection\textsuperscript{5,10,14,15}. For diffuse midline glioma, a BS-HGG with aggressive progression and overall survival of less than 1 year, contrast enhancement was only detected in 0%-25% of cases\textsuperscript{1}.

The application of MRP combined with MRS has the potential to overcome the limitations of conventional MRI. However, very few studies have examined the use of these two sequences for BSG grading. The only previous study examining these sequences in the literature was the study by Goda et al\textsuperscript{13}, which examined 20 BSG cases; however, only 8 cases had histopathological results, and the authors used the radiological prognostic index to classify tumors instead of histopathological grading. Our study used MRP and MRS for BSG grading and compared these outcomes with those based on pathological examinations for all 12 patients. This study is also the first to use ROC curve analysis to establish cutoff values for age, rCBV, rCBF, Cho/NAA, and Cho/Cre for use in BSG grading and diagnosis (Tables III and IV).

MRP assesses the extent of angiogenesis, which can provide a definitive diagnosis of brainstem tumors by differentiating tumors from non-tumor lesions and evaluating malignancy. Liu et al\textsuperscript{16} studied the application of DSC perfusion to 16 cases of non-enhanced medullary lesions and showed that the maximum rCBV of BSG (1.56) was significantly higher than that of non-tumor lesions (0.5; \( p < 0.001 \)). The study by Goda et al\textsuperscript{13} revealed that MRP had Se and Sp values of 100% and 100%, respectively, for the diagnosis of BS-HGG, compared with the respective corresponding values of 50% and 50% for conventional MRI sequences. In our study, BS-LGG and BS-HGG had respective rCBV values of 2.77 ± 1.33 and 8.53 ± 6.21 (\( p = 0.025 \)) and rCBF values of 2.27 ± 1.27 and 7.97 ± 4.67 (\( p = 0.016 \)). Overall, the rCBV values for

![Figure 5](https://example.com/figure5.png)

**Figure 5.** Receiver operating curve (ROC) analysis for age in the differentiation between high-grade and low-grade brainstem glioma. AUC = 0.889.
BSG were significantly higher than those reported for general gliomas. In the study by Metellus et al\(^8\), the mean rCBV of low-grade glioma was 0.84 ± 0.61. Many studies recommend using a cutoff rCBV value of 3 to differentiate between low-grade and high-grade glioma\(^8,19\). Jain et al\(^18\) that an rCBV cutoff value of 3 had 97.2% Se and 100% Sp for glioma grading. In the present study, we performed BSG grading using an rCBV cutoff value of 3.16, which resulted in a Se of 100%, a Sp of 66.7%, and an AUC of 0.889; for rCBF, the cutoff value of 3.56 had a Se of 83.3%, a Sp of 100%, and an AUC of 0.917 (Table IV). The cutoff values for distinguishing BSG grades were generally higher than those reported for general gliomas\(^8,19\).

MRS is a noninvasive diagnostic method capable of quantifying tumor tissue metabolism by measuring the concentrations of metabolites, which can be used to evaluate malignancy\(^20\). Low-grade glioma is often characterized by high concentrations of NAA, low concentrations of Cho, and the absence of lactate and lipid peaks. By contrast, high-grade glioma often shows low NAA levels due to neuronal degeneration or the destruction of neuronal structures in the tumor tissue. Glioblastoma (grade IV) is often characterized by necrosis with high concentrations of lipids and lactate peaks\(^20\). MRS performed on brainstem lesions has several challenges, including the proximity of bone, abundant vasculature, and the movement of cerebrospinal fluid, which can introduce heterogeneity in the primary magnetic field and difficult shimming\(^21\). However, Mascalchi et al\(^21\) demonstrated that single-voxel MRS is clinically feasible for assessing lesions of the midbrain and pons. Previous studies also confirmed a role for MRS in the diagnosis of brainstem tumors. Smith et al\(^22\) examined 34 patients with solitary brainstem lesions and reported that the Cho/Cr ratio in neoplastic lesions (2.0 ± 0.2) was significantly higher than that in non-neoplastic regions (1.4 ± 0.2). The study by Laprie et al\(^23\) reported Cho/NAA and Cho/Cr ratios in pediatric patients with diffuse midline gliomas of 3.8 ± 0.93 and 3.55 ± 1.37, respectively, which were significantly higher than the ratios in the normal brain region (\(p < 0.001\)). Multivoxel MRS performed in our study revealed increased Cho/NAA and Cho/Cr ratios in all patients. The respective Cho/NAA and Cho/Cr ratios of BS-LGG cases were 2.49 ± 1.09 and 5.37 ± 2.81, whereas the ratios for BS-HGG cases were 2.44 ± 0.47 and 4.33 ± 1.77 (Table III). The Cho/NAA ratio has a better diagnostic ability for tumor grading than the Cho/Cr ratio (\(p = 0.01\)). This result is similar to a previous study by Salmaggi et al\(^6\), which reported an increased Cho/Cr ratio in only 88.9% of cases, whereas 100% of cases were associated with an increased Cho/NAA ratio.

According to Law et al\(^24\), glioma grading using a Cho/Cr cutoff value of 1.08 had a Se of 97.5% and a Sp of 12.5%, whereas a Cho/NAA cutoff value of 0.75 had a Se of 96.7% and an Sp of 10%. In the present study, we performed ROC curve analysis to establish appropriate cutoff values. A Cho/Cr cutoff value of 3.08 has 83.3% Se and 100% Sp for BSG grading, with an AUC of 0.917. A Cho/NAA cutoff value of 3.88 has 83.3% Se and 100% Sp for BSG grading, with an AUC of 0.944 (Table IV). The Cho/NAA ratio had the highest diagnostic value, followed by the Cho/Cr ratio, rCBF, and rCBV (Figure 1).

Limitations

Our study has some limitations. First, the small sample size could introduce bias in the assessment of diagnostic efficiency. Second, using multivoxel MRS for small lesions in the brainstem might influence metabolite concentrations, leading to inaccurate quantitative metabolite ratios. Last, BSG characteristics differ between adults and children, and the combined assessment of these two groups may affect the research results. Therefore, further studies using larger study populations and separate evaluations of adult and pediatric patients may improve the diagnostic accuracy of these measurements.

Conclusions

Our study indicates that rCBF, rCBV, and the Cho/NAA and Cho/Cr ratios obtained by comparing solid tumors with the normal brain parenchyma may be useful for differentiating between BS-LGG and BS-HGG. The combination of MRP and MRS can provide vital information for treatment planning and prognosis in patients with BSG.

Ethical Approval

Ethical clearance was received from the Institutional Ethics Committee of Hanoi Medical University (Ref: 634/GCN-HDDDNCYSH-DHYHN dated 16 March 2022).

Informed Consent

The informed consent of patients was waived.
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Availability of Data and Material
The datasets generated and/or analysed during the current study are not publicly available due to privacy concerns but are available from the corresponding author on reasonable request.

Conflicts of Interest
The authors declare no conflict of interests.

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Authors’ Contributions
D.-H. Nguyen and M.-D. Nguyen prepared, drafted, and revised the manuscript critically, for important intellectual content. D. Tran and D.-H. Nguyen contributed substantially to the acquisition, analysis, and interpretation of data. Each author gave final approval to the version of the manuscript submitted for publication and agreed to be accountable for all aspects of the work, ensuring that questions related to the accuracy or integrity of any part of the work are appropriately investigated and resolved.

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References


